# Development of Biomimetic Surfaces by Vesicle Fusion

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### Introduction



A.F. Horwitz, Scientific American, May 1997.

#### Fibronectin - Integrin System



Image adapted from Leahy, D.L. et al., 1996, Cell 84:155

# Motivation

#### Intelligent Biomaterials:

- Minimize non-specific interactions with ECM
- Allow selective interaction with cells
  - Mimic ECM (Biomimetics)



#### Design Goals:

- Control Microenvironment of Cells
- Direct Cell Behavior

# Surface Biofunctionalization

#### Arrange Ligands on Surface:

- Accessibility
- Conformation
- Concentration
- Lateral Motion

#### Peptide Ligand

Polar Headgroup (small)

H/C Tails (bulky)



#### Properties of Lipid Bilayers: •Bending easier than stretching

Benaing easier than stretching
Flip flop times are high (10<sup>2</sup>-10<sup>5</sup> s)
Residence time (10<sup>4</sup> s)



**Compression Isotherm** 



# Vesicle Fusion



# Ellipsometry



### Refractive Index of a Single Bilayer



Assuming n of one DMPC Bilayer  $\cong$  n of one Monolayer (N=28)

$$\Delta z = 40 \text{\AA} \text{ (for } \Delta y_{max} = 0.035)$$

$$\square$$
Good Coverage
Headgroup Area of DMPC 59 \text{\AA}^2 \implies \Gamma\_{M} = 3.8 \text{ mg/m}^2

#### The Model

(From "Self Assembly Driven by Hydrophobic Interactions at Alkanethiol Monolayers: Mechanism of Formation of Hybrid Bilayer Membranes", J. B. Hubbard, V. Silin, A. L. Plant, Biophysical Chemistry 75 (1998) 163-176)



Mixed Boundary Condition:



- Where K: adsorption rate constant of mass (cm/s)
  - $C_{o}$ : bulk concentration of lipids (mg/ml)
  - D: diffusion coefficient of mass close to surface (cm<sup>2</sup>/s)

$$\left| \mathbf{J} \right|_{\text{Surface}} = \mathbf{K} \cdot \mathbf{C}_{o} \cdot \mathbf{e}^{\frac{\mathbf{K}^{2} \cdot \mathbf{t}}{\mathbf{D}}} \cdot \operatorname{erfc}(\frac{\mathbf{K}}{\mathbf{D}^{1/2}} \cdot \mathbf{t}^{1/2})$$

#### General and Limiting Cases

$$\frac{d\Gamma}{dt} = \beta \cdot J\Big|_{\text{surface}} = \left[1 - \frac{\Gamma(t)}{\Gamma_{M}}\right] \cdot J\Big|_{\text{surface}}$$

IC:  $\Gamma(t=0) = 0$ 

General Solution:

$$\Gamma(\mathbf{t}) = \Gamma_{M} \cdot \{1 - e^{-\frac{K \cdot C_{o}}{\Gamma_{M}} [\frac{D}{K^{2}} (e^{\frac{K^{2}t}{D}} \cdot \operatorname{erfc} \sqrt{\frac{K^{2}t}{D}} - 1) + \frac{2}{K} \cdot \sqrt{\frac{Dt}{\pi}}] \}$$

Characteristic Time of Adsorption:  $\tau = D/K^2$ 

For t/T >> 1 (Diffusion Limited Case): 
$$\Gamma(t) = \Gamma_M \cdot (1 - e^{-\frac{C_o}{\Gamma_M}(2\sqrt{\frac{D \cdot t}{\pi}} - \frac{D}{K})})$$

For t/t << 1 (Adsorption Limited Case):

$$\Gamma(t) = \Gamma_{M} \cdot (1 - e^{-\frac{K \cdot C_{o} \cdot t}{\Gamma_{M}}})$$

# Results

(Limiting Cases Fittings)



#### Effect of Peptide Amphiphile Presence on the Kinetics





10% mole PA DMPC

Case	Adsorption rate constant <i>K</i> , cm s <sup>-1</sup>	Diffusion coefficient D, cm² s <sup>-1</sup>
Diffusion Limited		7.4×10 <sup>-8</sup>
Adsorption Limited	1.4×10 <sup>-5</sup>	

Kinetics not Interrupted by PA presence

### Fluorescence Visualization



1,2-dihexadecanoyl-*sn*-glycero-3- phosphoethanolamine, triethylammonium salt (Texas Red<sup>®</sup> DHPE - Molecular Probes)







## PA for Cell Adhesion

- Controls the presentation of RGD, a peptide sequence important for cell adhesion, i.e vesicles, bilayers, etc.
- Focused on two peptide amphiphiles with different spacer groups,  $C_2$  and polyethylene oxide (PEO).



### **Experimental Procedure**



# Adhesion & Spreading Evaluation

- Inertia motion caused by mild microscope stage shaking determines adhesion.
- Scion Imaging software is used to determine the "shape factor."



#### Results EggPC Bilayer







#### Average Shape Factor- 0.86 (4 hours) No Adhesion

#### Results 10% C2-RGD Bilayer





Average Shape Factor- 0.84 (3 hours) No Adhesion

#### Results 10 % PEO-RGD Bilayer



#### **Concentration Effect**



#### 5% PEO-RGD

#### 10% PEO-RGD

(2 hours) Adhesion

### Surface Concentration Gradients

- Supported bilayers present a physically relevant substrate to study cell-ECM protein interactions
- Active protein sequences can be presented in a control manner using peptide amphiphiles
- There is a drive for the development of multifunctionalmulticomponent surfaces
- Further understanding of how specific ligand-integrin interactions modulate cell function is required
- Gradients of membrane bounded ligands can provide a useful tool to study this problem
- Vesicle fusion is the most efficient method to make surface gradients in a membrane environment

#### Ligand Concentration - Cell Spreading



**Figure:** NIH3T3 cells cultured on supported membranes after 4 hours. Membranes in (A) & (B) are 99% EggPC and 1% Texas Red DHPE while in (C) & (D) 94% EggPC, 5% (C16)2-Glu-PEO-GRGDSP and 1% Texas Red DHPE. Pictures (A) and (C) are in optical mode, while (B) and (D) in fluorescent mode on the same surface spot respectively.

### Ligand Concentration - Cell Migration



a. Uniform chemical concentration: Random motility only (µ)



 b. Migration in a chemical attractant gradient: Random motility (μ), chemokinesis (<sup>dμ</sup>/<sub>d</sub>) and chemotaxis (χ)



MICROSCOPY RESEARCH AND TECHNIQUE 43:358-368 (1998)

#### Steps to a Concentration Gradient

Barriers



Patterning



### Different ways to make barriers

#### Materials:

- Au, Al, Cr, Ti
- $Al_2O_3$ ,  $TiO_2$
- Fibronectin, BSA
- Polymerized Bilayers



Chemical Nature of Barrier - not topography - Blocks Diffusion

#### Techniques:

- ✓ Standard Photolithography (metals)
- Polymerization
- Microcontact Printing Spread - Neutral and Low PH
- Deep Abrasion (R<<10 nm)</li>

"Micropattern Formation in Supported Lipid Membranes", Jay T. Groves and Steven G. Boxer, Acc. of Chem. Res., 35, 149-157 (2002).

#### Chrome Grid



### Different ways to pattern

Photolithographic Patterning (Photoactivatable peptides)

#### Microprinting

![](_page_27_Figure_3.jpeg)

![](_page_27_Figure_4.jpeg)

#### Direct Pipetting

#### **Microfluidic Flow**

![](_page_27_Picture_7.jpeg)

"Micropattern Formation in Supported Lipid Membranes", Jay T. Groves and Steven G. Boxer, Acc. of Chem. Res., 35, 149-157 (2002).

#### Microfluidic Networks

![](_page_28_Figure_1.jpeg)

**Figure 2.** Fluorescence micrographs showing (b) linear and (c, d) parabolic gradients of fluorescein in solution. The microfluidic network we used for generating these gradients had 3 inlets and 9 outlets (a). The concentration of the solutions we introduced into each inlet of our microfluidic network is indicated above the micrographs. The plots below the micrographs show the corresponding fluorescence intensity profile (green line) across the broad channel (900  $\mu$ m wide) 500  $\mu$ m downstream (L, white dotted line) from the junction. The theoretically calculated concentration profiles of fluorescein are shown as black, round dots. The gray lines and dots in the graphs show the calculated contribution of the individual inputs to the overall profile. The flow rate in the broad channel is 1 mm/s.

Anal. Chem. 2001, 73, 1240-1246

#### Construction

![](_page_29_Figure_1.jpeg)

![](_page_29_Figure_2.jpeg)

### Evaluation

![](_page_30_Picture_1.jpeg)

![](_page_30_Figure_2.jpeg)

![](_page_30_Figure_3.jpeg)

![](_page_30_Figure_4.jpeg)

## SEM

![](_page_31_Picture_1.jpeg)

![](_page_31_Picture_2.jpeg)

![](_page_31_Figure_3.jpeg)

![](_page_31_Picture_4.jpeg)

# Testing

![](_page_32_Picture_1.jpeg)

![](_page_32_Picture_2.jpeg)

![](_page_32_Figure_3.jpeg)

![](_page_32_Figure_4.jpeg)

## Conclusions

- Ellipsometry was used to study the kinetics of VF on SiO<sub>2</sub>
- Bilayer formation from vesicles is adsorption limited
- Fluorescence microscopy was used to visualize the membranes
- Peptide accessibility and density are important for cell binding
- Surface composition gradients are useful in studying cellular function modulation induced by ligand-integrin interactions on a biomimetic membrane
- A novel technique was developed to control the microenvironment of cells in 2-D

![](_page_33_Picture_7.jpeg)

#### Acknowledgments

Dr. Alejandro Parra Dr. Haining Zhang PEO chemistry

Clean-room Processing

This work was partially supported by the MRSEC Program of the National Science Foundation under Award No. DMR00-80034, the National Science Foundation NIRT Award No. CTS-0103516, and the Army Research Office through the Institute for Collaborative Biotechnologies.

Ning Cao

Ellipsometry